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<p>(21) International Application Number: PCT/US99/20530 (22) International Filing Date: 7 September 1999 (07.09.99) (30) Priority Data: 09/218,336 21 December 1998 (21.12.98) US (71) Applicant: LIGHT SCIENCES LIMITED PARTNERSHIP [US/US]; 1065 - 12th Avenue N.W. #E5, Issaquah, WA 98027 (US). (72) Inventor: CHEN, James, C.; 2011 - 87th Place N.E., Bellevue, WA 98004 (US). (74) Agent: ANDERSON, Ronald, M.; Law Offices of Ronald M. Anderson, Suite 507, 600 - 108th Avenue N.E., Bellevue, WA 98004 (US).</p>		<p>(81) Designated States: AU, CA, JP, European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE). Published With international search report.</p>
<p>(54) Title: PEGYLATED PHOTSENSITIZERS FOR ABNORMAL TISSUE TREATMENT</p> <div data-bbox="349 1108 1284 1549"><p>Diagram illustrating a microparticle conjugate. The central shaded circle is labeled "MICROPARTICLE". It is surrounded by a dashed circle labeled "POLYMERIC COATING". On the coating, there are several small circles labeled "18" representing "PHOTOSENSITIVE AGENT". There are also wavy lines labeled "20" representing "ANTIBODY LINK SITE". A label "10a" points to the entire assembly.</p></div> <p>(57) Abstract</p> <p>A photosensitizer (18) suitable for use in administering photodynamic therapy (PDT), conjugated with antibodies that are targeted to antigens on abnormal tissue, and polyethylene glycol (PEG) or other polymer that extends the residence time of the conjugate (64) within a patient's body. The resulting pegylated targeted conjugate (64) is administered to a patient, and after the antibodies have had sufficient time to bind with the antigens, light from an external or internal source having a waveband corresponding to an absorption waveband of the photosensitizer (18) is administered. Use of an external light source that emits relatively long wavelength light enables the light to pass through any intervening dermal layer, and normal tissue between the external light source, and the treatment site. Since the photosensitizer (18) in the conjugate (64) is bound to the abnormal tissue, the light therapy has minimal effect on the intervening normal tissue.</p>		

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PEGYLATED PHOTSENSITIZERS FOR ABNORMAL TISSUE TREATMENT**Field of the Invention**

5 The present invention is generally related to the use of light therapy to destroy abnormal tissue that has absorbed a photosensitizer, and more specifically, to the use of a photosensitizer that is targeted to bind with the abnormal tissue, but not normal tissue, so that the light administered during the therapy has a minimal adverse effect on surrounding normal tissue, which is generally free of the photosensitizer.

10 Background of the Invention

Abnormal tissue in the body is known to selectively absorb certain photosensitizer dyes that have been administered to a patient to a much greater extent than normal tissue surrounding a treatment site. For example, tumors of the pancreas and colon may absorb two to three times the volume of these dyes, compared to normal tissue. The cancerous or abnormal tissue that has absorbed the photosensitizer dye can then be destroyed by administering light of an appropriate wavelength or waveband corresponding to an absorbing wavelength or waveband of the photosensitizer dye. This procedure, which is known as photodynamic therapy (PDT), has been clinically used to treat metastatic breast cancer, bladder cancer, lung carcinomas, esophageal cancer, basal cell carcinoma, malignant melanoma, ocular tumors, head and neck cancers, and other types of malignant tumors. Because PDT may selectively destroy abnormal tissue that has absorbed more of the dye than normal tissue, it can successfully be used to kill the malignant tissue of a tumor with less effect on surrounding benign tissue than alternative treatment procedures, such as traditional chemotherapy or radiation therapy.

25 However, even those photosensitizers that are much more selectively absorbed by abnormal tissue will still be absorbed to some lesser extent by the

normal tissue of a patient's body. If the light therapy administered is limited primarily to the abnormal tissue at the treatment site so that very little light is applied to the adjacent normal tissue, which has absorbed the photosensitizer to a lesser extent, the effect of the light therapy on such normal tissue will be minimal.

5 To enable the selective application of light therapy to an internal treatment site with minimal exposure of surrounding normal tissue, it is typically necessary to either surgically expose the internal treatment site, or insert an appropriate light source probe into the patient's body and advance it to the treatment site, for example, using conventional endoscopic procedures, or insert a light source probe
10 interstitially into a tumor.

More recently, techniques have been developed for administering light therapy to an internal treatment site from an externally disposed light source. These techniques take advantage of the fact that light having a relatively long wavelength will readily penetrate dermal tissue to activate photosensitizers
15 absorbed by abnormal tissue at an internal treatment site. The disadvantage of this approach is that normal tissue lying between the light source and the internal treatment site is also irradiated by the light as it passes through the overlying tissue to the internal treatment site. Skin and other normal tissue in the propagation path of the light administered externally to render PDT to an internal
20 treatment site will thus be adversely affected by the therapy. The effects of the light therapy on normal tissue that has absorbed the photosensitizer may range from mild reddening of the skin to severe damage to the normal dermal tissue. Clearly, it would be desirable to minimize damage to the normal tissue by substantially reducing the extent to which the normal skin and tissue absorb the
25 photosensitizer.

One approach developed to address the preceding problems is to bind antibodies to a photosensitizer that are targeted to the abnormal cells at a treatment site. When a photosensitizer conjugated with an antibody is administered to a patient, the antibodies will tend to bind the photosensitizer to the
30 abnormal tissue, but not to normal tissue, thereby improving the specificity of the PDT and avoiding harm to the normal tissue. However, it has been shown that targeted photosensitizers that are conjugated with an antibody can have a relatively low uptake by abnormal tissue in a tumor. In some cases, as little as 0.1% of an injected dose of photosensitizer is actually absorbed by the abnormal
35 cells in a tumor. The low tumor uptake of antibody targeted photosensitizers (or other drugs) is due in part to the rapid plasma clearance by the reticuloendothelial

system and poor penetration of the targeted conjugate across vascular endothelium. In effect, the targeted photosensitizer is cleared too rapidly from the plasma in the patient's body to have an opportunity to bind the antibody with the abnormal tissue at the levels desired.

- 5 More generally, too rapid clearance of conventional photosensitizers (i.e., a non-targeted photosensitizer) from plasma has also been recognized as problem. One solution that has been explored is the use of a synthetic drug carrier such as polyethylene glycol (PEG). As previously reported by others, PEG coated microparticulates containing a photosensitizer (zinc phthalocyanine) have been
10 tested *in vivo*. In addition, V.P. Torchilin has published an article entitled, "Polymer-coated Long-Circulating Microparticulate Pharmaceuticals," in Journal Microencapsulation, vol. 15, no. 1, (1998) pp. 1-19, in which he discusses the protective effect of certain polymers, including PEG, on nanoparticulate drug carriers, including micelles, for extending the circulation time of the encapsulates
15 in solution. PEG is well known as a sterically protecting polymer and drug carrier. Useful biological properties of PEG include its water solubility, low immunogenicity, and extended life while circulating in mammalian organisms. A PEG dextran conjugate has been used as a combined stabilizer and surface modifier to produce resorbable poly(DL-lactide-co-glycolide) (PLG)
20 microparticles by an emulsification/solvent technique as described by A.G.A. Coombes et al. in "Biodegradable Polymeric Microparticles for Drug Delivery and Vaccine Formulation: the Surface Attachment of Hydrophilic Species Using the Concept of Poly(ethylene glycol) Anchoring Segments," in Biomaterials 1997, vol. 18, No. 17, page 1153. However, it appears that protectively polymerized
25 drugs have not been conjugated with antibodies that can target the drugs to abnormal tissue. Clearly, the combination of a polymer such as PEG to protect a photosensitizer that is conjugated with an antibody could solve both the too rapid clearing of conventional targeted photosensitizer conjugates from the plasma and ensure that the photosensitizer binds only to the abnormal tissue, to substantially
30 eliminate any damage to the normal tissue by the light therapy. Such a combination has not been disclosed or suggested by the prior art.

Summary of the Invention

- In accord with the present invention, a method for destroying abnormal tissue within a patient's body is defined. The method includes the step of
35 providing a photosensitizer that is characterized by absorbing light within a defined waveband. The photosensitizer is sterically protected by a polymer and is

conjugated with an antibody that is targeted at the abnormal tissue, producing a polymer protected antibody/photosensitizer conjugate. When the polymer protected antibody/photosensitizer conjugate is administered to the patient, the antibody portion of the conjugate preferentially links with the abnormal tissue at the treatment site, while the polymer increases an *in vivo* residence time of the antibody/photosensitizer conjugate within the patient's body. Consequently, there is an increased uptake of the antibody/photosensitizer conjugate by the abnormal tissue at the treatment site. Light within the defined waveband is administered to the internal treatment site, thereby activating the photosensitizer to destroy the abnormal tissue.

The polymer in the above-described method is preferably polyethylene glycol or a derivative of polyethylene glycol and is water soluble, hydrophilic, and biocompatible. In addition, the polymer exhibits a low toxicity and a low immunogenicity, is not biodegradable, and does not form any toxic metabolites. Other desired characteristics of the polymer include a high enough molecular weight, combined with a highly flexible main chain to provide for long *in vivo* residence times in a human body. The polymer should have at least one attachment site to which the photosensitizer and antibody may be covalently bonded.

The wavelengths of the light used when administering the light therapy from an external source are sufficiently long to readily pass through a dermal layer and through intervening tissue to reach the internal treatment site. Instead of being administered externally, the light may be administered internally using a light source disposed interstitially so that the light is administered to the treatment site within a patient's body.

The treatment site may be localized, such as at a tumor, or it may be disseminated throughout at least a portion of the patient's body, and the abnormal tissue may be distributed throughout the treatment site. The treatment site may include at least part of a vascular system of the patient in which the abnormal tissue is disposed. Furthermore, the abnormal tissue may be a tumor, non-localized malignant cells, or may be a disease causing bacteria or a disease causing virus.

The method described above may serve as a prophylaxis by administering the polymer protected antibody/photosensitizer conjugate and administering light to a prospective treatment site at which abnormal tissue may possibly develop.

This prophylactic treatment may be repeated at intervals to prevent development of the abnormal tissue within the patient.

It is also contemplated that the method described above may be used following the surgical removal of a substantial portion of the abnormal tissue, to
5 destroy any residual abnormal tissue at the treatment site, or following the transplanting of bone marrow into a patient, to destroy residual abnormal tissue in the patient's body.

Another aspect of the present invention is directed to a method to improve a specificity with which a photosensitizer is taken up by abnormal cells within a
10 patient. In this further aspect of the invention, a microparticle, a photosensitizer, an antibody that is targeted at antigens on the abnormal cells, and a polymer are provided. The antibody and the photosensitizer are conjugated to the microparticle, and the microparticle is coated with a polymer that prolongs an *in vivo* residence time for the microparticle based antibody/photosensitizer conjugate. When the
15 polymer coated microparticle based antibody/photosensitizer conjugate is administered to a patient, the antibody on the conjugate links with the abnormal cells. The linking action of the antibody and ability of the polymer coating to increase the *in vivo* residence time results in a higher uptake of the polymer coated microparticle based antibody/photosensitizer conjugate by the abnormal cells than
20 would be possible using a microparticle based antibody/photosensitizer conjugate that is not coated with the polymer.

The microparticle may comprise a micelle. Preferably, the polymer is PEG.

Brief Description of the Drawing Figures

25 The foregoing aspects and many of the attendant advantages of this invention will become more readily appreciated as the same becomes better understood by reference to the following detailed description, when taken in conjunction with the accompanying drawings, wherein:

FIGURE 1 schematically illustrates a first form of a polymer protected
30 antibody/photosensitizer conjugate microparticle;

FIGURE 2 is a schematic view showing the polymer protected antibody/photosensitizer conjugate of FIGURE 1 bound to a target malignant cell organelle by the antibody;

FIGURE 3A schematically illustrates a second form of a polymer
35 protected antibody/photosensitizer conjugate in which a photosensitizing agent and an antibody are bonded to a polymer at separate attachment sites;

FIGURE 3B schematically illustrates a third form of a polymer protected antibody/photosensitizer conjugate in which a photosensitizing agent and an antibody are bonded to a polymer at the same attachment site;

FIGURE 4 is a schematic view of the third form of a polymer protected antibody/photosensitizer conjugate bound to a target malignant cell organelle by the antibody;

FIGURE 5 is a schematic cross-sectional view of a portion of a patient's body in which a blood vessel is disposed, showing the polymer protected antibody/photosensitizer conjugates being injected into the patient's bloodstream with a syringe;

FIGURE 6 is a schematic cross-sectional view of a portion of a patient's body containing a tumor, showing an external long wavelength light source being used to activate the photosensitizers in the polymer protected antibody/photosensitizer conjugates that are linked to the abnormal tissue in the tumor; and

FIGURE 7 is a schematic cross-sectional view of a portion of a patient's body containing a tumor, showing an internal light source being used to activate the photosensitizers in the polymer protected antibody/photosensitizer conjugates that are linked to the abnormal tissue in the tumor.

Description of the Preferred Embodiment

Polymer Protected Antibody/Photosensitizer Conjugates

Referring to FIGURE 1, a polymer protected antibody/photosensitizer conjugate 10a in accordance with the present invention is schematically illustrated. Polymer protected antibody/photosensitizer conjugate 10a includes a microparticle core 12 of the type normally used as a drug carrier. It is contemplated that the microparticle may be a micelle or a carrier, such as a latex sphere. Other inert, biocompatible microparticles may be used for the core or carrier. The choice of the particular microparticle will be determined by a number of factors, including the chemical compatibility of the microparticle with the antibody, the photosensitizer, and the polymer.

Attached to the surface of microparticle core 12 are a plurality of antibody linking sites 20, which are specifically targeted to link with antigens on abnormal tissue, or malignant cell organelles, or disease causing organisms within a patient's body. Note that as used herein and in the claims that follow, unless otherwise evident from the context, the term "abnormal tissue" is intended to encompass malignant cell organelles and disease causing organisms. Also

attached to the surface of microparticle core 12 are a plurality of photosensitizers 18 of the type suitable for use in administering PDT.

5 Microparticle core 12 is coated with a polymer 16. Polymer 16 increases the *in vivo* residence time of the antibody/photosensitizer conjugates within the patient's body, e.g., within the plasma, allowing a lower dose of the photosensitizer conjugate to be used, while simultaneously increasing the uptake of the antibody/photosensitizer conjugate by the abnormal tissue. Polymer 16 is preferably polyethylene glycol (PEG) or PEG based, having a moderately high molecular weight, e.g., on the order of 20,000. Other polymers that exhibit
10 similar properties may also be used to extend the residence time of the photosensitizer targeted conjugate within the patient's body. The polymer selected for this purpose must be: water soluble, hydrophilic, biocompatible, must exhibit a low toxicity, and must have a low immunogenicity. In addition, the polymer must not be biodegradable or form any toxic metabolites, must have a
15 sufficiently high molecular weight, coupled with a highly flexible main chain, to provide for relatively long *in vivo* residence times in a human body, e.g., for more than several hours, and must be chemically compatible with the photosensitizer and antibody used for the conjugate.

 An understanding of how the polymer coating results in longer *in vivo* residence times is helpful in designing a microparticle based polymer protected antibody/photosensitizer conjugate in accord with the present invention. Polymer 16 comprises a long, highly flexible main chain and has a moderately high molecular weight (which means that the main chain is longer in length than most molecules). The flexible main chain is in constant motion, creating a
25 "cloud," which protects the surface of the microparticle and dramatically increases *in vivo* residence times. However, this same "cloud" may also tend to inhibit antibody link sites 20 from successfully binding with corresponding antigens on the target abnormal tissue. The prior art teaches that relatively minor amounts (1-2 mol%) of a polymer such as PEG provide sufficient protection to increase *in vivo* residence time, while higher concentrations tend to inhibit antibody linking.
30 It is therefore anticipated that the optimal concentration of polymer used in producing a conjugate will need to be empirically determined for each different microparticle based polymer protected antibody/photosensitizer conjugate species.

 FIGURE 2 illustrates how targeted polymer protected
35 antibody/photosensitizer conjugate 10a is used for destroying a malignant cell organelle 22. In this Figure, targeted polymer protected antibody/photosensitizer

conjugate 10a is shown with one of the antibody link sites 20 linked to an antigen 24 that is associated with the malignant cell organelle. Because normal cells do not have any antigen to which antibody link sites 20 will bind, targeted polymer protected antibody/photosensitizer conjugates 10a do not become bound to normal cells. After providing sufficient time for the targeted polymer protected antibody/photosensitizer conjugates to bind to the malignant cell organelles or other types of abnormal tissue within a patient's body, a light 154 having a waveband corresponding to a characteristic light absorption waveband of the photosensitizer is applied using one of the techniques disclosed hereinbelow. This light activates a photosensitizer 18, causing it to form new chemical species, such as free oxygen radicals, which attack the target malignant cells or other abnormal tissue.

FIGURES 3A and 3B illustrate forms of polymer protected antibody/photosensitizer conjugates, which do not incorporate a microparticle core. In these embodiments, the antibody/photosensitizer conjugate is covalently bonded to the polymer rather than being attached to a microparticle. FIGURE 3A illustrates polymer protected antibody/photosensitizer conjugate 10b in which photosensitizer 18 is covalently bonded to one attachment site of polymer 26a, while the antibody which includes antibody link site 20 is covalently bonded to a different attachment site of polymer 26a. Polymer 26a is preferably PEG, which has one attachment site at each end of the polymer chain.

FIGURE 3B illustrates polymer protected antibody/photosensitizer conjugate 10c in which photosensitizer 18 is covalently bonded to one attachment site of polymer 26b, while the antibody which includes antibody link site 20 is covalently bonded to photosensitizer 18. Polymer 26b is preferably methyl-PEG, a PEG derivative which has only a single attachment site at one end of the polymer chain; the other attachment site having been replaced with a methyl group.

For the two forms of the polymer protected antibody/photosensitizer conjugate respectively illustrated in FIGURES 3A and 3B, it is important that antibody link site 20 be positioned in such a manner as to allow it easy access to corresponding antigen 24 on the targeted malignant cell organelle or other abnormal tissue, as illustrated in FIGURES 2 and 4. The relative positions of polymers 26a and 26b, antibody link site 20, and photosensitizer 18, as shown in FIGURES 3A and 3B, are not the only possible configurations. Actual positional configurations of the conjugates will be a function of the polymer chosen and the

attachment sites available. Some polymers have a plurality of attachment sites available, thus a plurality of antibody link sites 20 and/or photosensitizers 18 may be covalently bonded to a single polymer molecule. The selection of polymer 26a or 26b will be based on the chemical compatibility of the polymer, antibody 20, and photosensitizer 18. Those skilled in the art will readily understand that appropriate chemical manipulations and processes will be required to form the desired polymer protected antibody/photosensitizer conjugate, and the ease or difficulty of such manipulations and processes will factor decisively in the ultimate configuration of the polymer protected antibody/photosensitizer conjugate employed.

FIGURE 4 illustrates how targeted polymer protected antibody/photosensitizer conjugate 10c is used for destroying a malignant cell organelle 22. In a manner similar that of FIGURE 2, targeted polymer protected antibody/photosensitizer conjugate 10c is shown with antibody link site 20 bound to an antigen 24. After providing sufficient time for targeted conjugates 10c to bind to the targeted abnormal tissue, light 154 of an appropriate waveband, i.e., corresponding to the absorption waveband of the photosensitizer, is applied using one of the techniques disclosed hereinbelow. The light activates photosensitizer 18, destroying the abnormal tissue.

Injection of Targeted Polymer Protected Antibody/Photosensitizer Conjugates

It is generally preferable to introduce the polymer protected antibody/photosensitizer conjugates as close as possible to a treatment site, such as by introducing the polymer protected antibody/photosensitizer conjugate directly into a tumor. At times, the location of a tumor or other treatment site is such that it is not feasible to localize the administration of the polymer protected antibody/photosensitizer conjugate. Furthermore, the targeted abnormal tissue may not be localized, but instead, may be viruses, microorganisms or metastasized cancer cells, which are more broadly distributed throughout a patient's body. It is therefore contemplated that polymer protected antibody/photosensitizer conjugates 10a, 10b, and 10c may be injected into the patient's bloodstream to allow the patient's own circulatory system to deliver the polymer protected antibody/photosensitizer conjugates to the targeted abnormal tissue. As illustrated in FIGURE 5, a syringe 58 can be used to inject a fluid containing the targeted polymer protected antibody/photosensitizer conjugates in suspension through a dermal layer 70 and into a bloodstream 72. A needle 60 passes through dermal layer 70 and through a wall 76 of bloodstream 72; fluid containing the targeted

polymer protected antibody/photosensitizer conjugates is injected through needle 60 into blood 74. The blood flow in the vessel carries the targeted polymer protected antibody/photosensitizer conjugates downstream, to one or more locations where the targeted abnormal tissue is disposed. It is important to note that antibody link sites 20 will seek out and bind only to the selected targeted abnormal tissue, which incorporates antigen 24, as shown in FIGURES 2 and 4. Since the photosensitizer is not linked to normal tissue, injury to normal tissue is minimized during administration of the light, particularly, if the light is administered from an external source and must pass through normal tissue to reach the abnormal tissue that has been targeted.

Activation of the Photosensitizer

The photosensitizer in the polymer protected antibody/photosensitizer conjugate destroys abnormal tissue to which it is bound when light of the proper waveband is administered. While the mechanism by which PDT destroys cells is not fully understood, it is believed to produce free oxygen radicals that are toxic to the abnormal tissue.

In FIGURE 6, a tumor 140 has been infused with polymer protected antibody/photosensitizer conjugates 64. These conjugates may be of the forms illustrated in FIGURES 1, 3A, or 3B (i.e., conjugates 10a, 10b, and 10c, respectively). The polymer protected antibody/photosensitizer conjugates can be infused either within a biocompatible fluid, such as a physiological saline solution, or can be applied topically to the exterior surface of tumor 140. Tumor 140 lies within the patient's body, adjacent a dermal layer 144. Outside the patient's body, a power supply 150 is coupled through a lead 148 to an external light array 146. Array 146 comprises a plurality of light sources 152 such as LEDs. When energized by power supply 150, light sources 152 emit light 154 of the desired wavelength that passes freely through the dermal layer and into tumor 140, activating photosensitizer 18 that is included within polymer protected antibody/photosensitizer conjugates 64, so that photosensitizer 18 produces substances that attack tumor 140.

FIGURE 7 illustrates yet another technique for exposing polymer protected antibody/photosensitizer conjugates 64 to light 154 of the waveband corresponding to the light absorption waveband of the photosensitizer. In this approach, a probe 160 is inserted interstitially within tumor 140. Probe 160 includes a linear array 162 of LEDs (or other appropriate light sources) that are energized through a lead 164. Lead 164 is coupled to a remote internal (or

external) power supply (not shown). If disposed internally, the power supply can be energized using an external power source that is electromagnetically coupled to the internal power supply. A detailed description of apparatus suitable for providing such electromagnetic coupling is provided in U.S. Patent
5 No. 5,715,837, which is assigned to the same assignee as the present invention, the disclosure and drawings of which are hereby specifically incorporated herein by reference.

As noted above, the targeted abnormal tissue may not be a localized tumor, but instead, may comprise metastasized cancer cells, disease causing
10 viruses, disease causing bacteria or other undesirable microorganisms that are distributed throughout at least a portion of the patient's body. In this instance, the light employed for administering the light therapy preferably has a relatively long wavelength, e.g., longer than 800 nm, to enable the light to pass through several cm. of tissue. Generally, the longer the wavelength of the light, the greater its
15 ability to penetrate tissue in the body of the patient. Of course, the light adsorption waveband of the photosensitizer must be matched to the wavelength or waveband of the light that is administered to activate the photosensitizer. It is contemplated that by passing a long wavelength light source over the external surfaces of a patient's body, the majority of the polymer protected
20 antibody/photosensitizer conjugates attached to targeted abnormal tissue may be activated, thus destroying the abnormal tissue, even though widely disseminated within the patient's body.

It is also contemplated that polymer protected antibody/photosensitizer conjugates can be employed prophylactically to prevent the development of
25 abnormal tissue at a prospective treatment site. For example, it is now possible to identify women with susceptibility to certain types of breast cancer based upon genetic testing. The probabilities of developing breast cancer in a women who has tested positive for the susceptible genes is so significant that some women choose to undergo prophylactic radical mastectomy to minimize the risk of later
30 developing breast cancer. Instead, the present invention can provide an alternative prophylaxis, by providing for repetitive administration of a polymer protected antibody/photosensitizer conjugate targeted at the type of cancerous tumor cells that might develop, followed by administration of light therapy using light having a waveband corresponding to the light adsorption waveband of the
35 photosensitizer. By periodically repeating such prophylactic therapy,

development of cancerous tumor cells in the woman's breast can likely be prevented, but without the trauma involved in undergoing a radical mastectomy.

Another application of the present invention is for destroying any residual abnormal tissue that may remain at a tumor resection site, following surgical removal of the tumor. A common problem following such surgery is the regrowth of the tumor. After administering a polymer protected antibody/photosensitizer conjugate targeted at antibodies of the tumor that was removed, light therapy can be administered to destroy the residual tumor cells that have linked with the conjugate, thereby preventing the regrowth of the tumor. Such post-surgical treatment might be rendered, for example, following a mastectomy or brain tumor removal.

Yet another application of the present invention is in the treatment of leukemia or other diseases requiring bone marrow transplant. A polymer protected antibody/photosensitizer conjugate targeted at malignant antigens in the bone marrow can be administered followed by administration of light therapy using light of the appropriate waveband, as noted above. This treatment should be effective both pre- and post-bone marrow transplant to destroy much of the abnormal tissue causing the leukemia, and may be employed, in addition to more conventional radiation and chemotherapy treatments. It is also contemplated that the present invention may be used for destroying abnormal tissue in bone marrow, thereby avoiding the need for a bone marrow transplant. The polymer protected antibody/photosensitizer conjugate may be activated with light administered either from an interstitial source or an external source, i.e., transcutaneously or from within the patient's body.

While empirical evidence such as may be developed by clinical trials of the present invention have not yet been provided, it is believed by some authorities that antibodies like those used in the polymer protected antibody/photosensitizer conjugate may activate the body's own immune system. Furthermore, photodynamic activation of a photosensitizer has been demonstrated to also cause an immune response. It is expected that the present invention will produce a synergistic effect in enhancing the efficacy of PDT that is far greater than either of these processes alone. The use of a polymer such as PEG to protect a targeted photosensitizer is also expected to provide a much greater improvement in the efficacy of the conjugate than might be expected relative to the use of a PEG photosensitizer conjugate alone or a targeted photosensitizer alone.

Although the present invention has been described in connection with the preferred forms of practicing it and modifications thereto, those of ordinary skill in the art will understand that many other modifications can be made within the scope of the claims that follow. Accordingly, it is not intended that the scope of
5 the invention in any way be limited by the above description, but instead be determined entirely by reference to the claims that follow.

The invention in which an exclusive right is claimed is defined by the following:

1. A method for destroying abnormal tissue in a patient, at an internal treatment site, comprising the steps of:

(a) providing a polymer protected antibody/photosensitizer conjugate, the photosensitizer portion characterized by absorbing light within a defined waveband, the polymer portion characterized by having a high molecular weight combined with a highly flexible main chain, thereby providing steric protection to the conjugate, and the antibody portion characterized by being targeted to an antigen which exists substantially only at the abnormal tissue in the patient;

(b) administering the polymer protected antibody/photosensitizer conjugate to the patient, said antibody linking with the abnormal tissue at the treatment site, and said polymer increasing an *in vivo* residence time of the antibody/photosensitizer conjugate to allow for an increased uptake of the antibody/photosensitizer conjugate by the abnormal tissue at the treatment site; and

(c) administering light within the defined waveband to the internal treatment site, said light activating the photosensitizer to destroy the abnormal tissue.

2. The method of Claim 1, wherein the polymer comprises polyethylene glycol.

3. The method of Claim 1, wherein the polymer comprises a derivative of polyethylene glycol.

4. The method of Claim 1, wherein the polymer is water soluble and hydrophilic.

5. The method of Claim 1, wherein the polymer is biocompatible, exhibiting a low toxicity and a low immunogenicity in a concentration administered to the patient.

6. The method of Claim 1, wherein the polymer must have at least one attachment site to which the photosensitizer and the antibody covalently bond.

7. The method of Claim 1, wherein the defined waveband includes wavelengths sufficiently long to readily pass through a dermal layer of the patient.

8. The method of Claim 7, wherein the light is administered externally to a body of the patient and passes through intervening tissue to reach the internal treatment site.

9. The method of Claim 8, wherein the abnormal tissue is distributed throughout at least a portion of a body of the patient.

10. The method of Claim 8, wherein the treatment site includes at least part of a vascular system of the patient, said abnormal tissue being disposed within said at least part of the vascular system.

11. The method of Claim 1, wherein the abnormal tissue includes at least one of a disease causing bacteria and a disease causing virus.

12. The method of Claim 1, wherein the step of administering the light includes the step of inserting a light source that emits light interstitially within the internal treatment site so that the light is administered to the internal treatment site.

13. The method of Claim 1, wherein the internal treatment site is a prospective treatment site at which abnormal tissue may possibly develop, further comprising the steps of:

- (a) administering the polymer protected antibody/photosensitizer conjugate to the patient; and
- (b) as a prophylaxis, administering the light to the prospective treatment site.

14. The method of Claim 13, wherein the steps of administering the polymer protected antibody/photosensitizer conjugate and administering the light as a prophylaxis are repeated at spaced-apart intervals of time to prevent development of the abnormal tissue at the prospective treatment site from occurring.

15. The method of Claim 1, further comprising the step of surgically excising a substantial portion of the abnormal tissue, followed by the steps of administering the polymer protected antibody/photosensitizer conjugate, and administering the light, to destroy any residual abnormal tissue at the treatment site.

16. The method of Claim 1, further comprising the step of transplanting bone marrow into the patient, followed by the steps of administering the polymer protected antibody/photosensitizer conjugate, and administering the light, to destroy residual abnormal tissue in the patient.

17. A method for improving a specificity and an extent with which a photosensitizer is taken up by abnormal tissue within a patient, compared to normal tissue, comprising the steps of:

(a) providing a microparticle, a photosensitizer, an antibody that is targeted at antigens of the abnormal tissue, and a polymer;

(b) conjugating said antibody and said photosensitizer to said microparticle, forming a microparticle based antibody/photosensitizer conjugate that is adapted to link with the abnormal tissue;

(c) coating said microparticle based antibody/photosensitizer conjugate with a polymer forming a polymer coated microparticle based antibody/photosensitizer conjugate that is characterized by a prolonged *in vivo* residence time for the microparticle based antibody/photosensitizer conjugate in the patient; and

(d) administering the polymer coated microparticle based antibody/photosensitizer conjugate to the patient, so that said antibody on the microparticle based antibody/photosensitizer conjugate links with the abnormal tissue, uptake of the polymer coated microparticle based antibody/photosensitizer conjugate by the abnormal tissue being substantially improved compared with a microparticle based antibody/photosensitizer conjugate that is not coated by the polymer and uptake of the polymer coated microparticle based antibody/photosensitizer conjugate by the normal tissue being substantially reduced compared with a microparticle based photosensitizer that is coated by the polymer.

18. The method of Claim 17, wherein the microparticle comprises one of a micelle and a substantially inert carrier core.

19. The method of Claim 17, wherein the polymer is polyethylene glycol.

20. A method for improving a specificity with which a photosensitizer is taken up by abnormal tissue within a patient, comprising the steps of:

(a) providing a photosensitizer, an antibody that is targeted at antigens present at the targeted treatment site, and a polymer that is water soluble, hydrophilic, of sufficiently high molecular weight, characterized by having a highly flexible main chain, which provides for an extended *in vivo* residence time in a human body, and capable of forming at least one covalent bond with the photosensitizer and antibody;

(b) conjugating the antibody and photosensitizer with the polymer to form a polymer/antibody/photosensitizer conjugate; and

(c) administering the polymer/antibody/photosensitizer conjugate to the patient, so that the antibody on the polymer/antibody/photosensitizer conjugate links with the abnormal tissue during the extended *in vivo* residence time, substantially improving uptake of the polymer/antibody/photosensitizer conjugate by the abnormal tissue.

21. The method of Claim 20, wherein the polymer is polyethylene glycol.

22. A method for enhancing an efficacy of a light therapy rendered to destroy abnormal tissue, comprising the steps of:

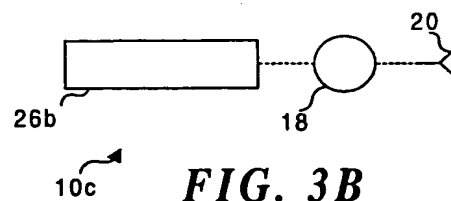
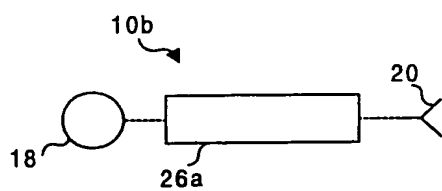
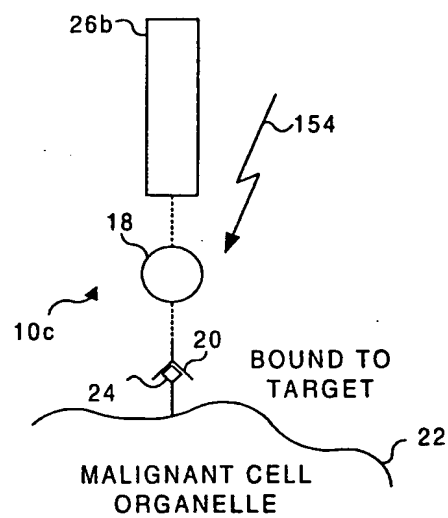
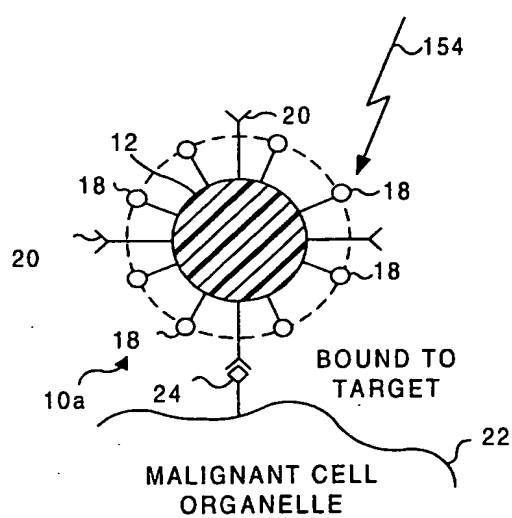
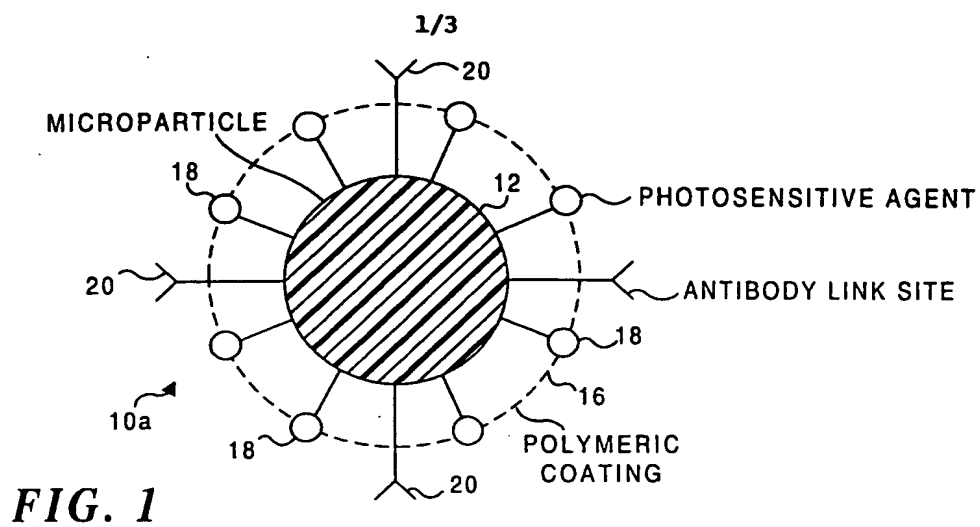
(a) administering polyethylene glycol (PEG) and a photosensitizer that is conjugated with an antibody targeted to bind with antigens present on the abnormal tissue, said polyethylene glycol serving to extend a viable lifetime of a resulting PEG/photosensitizer/antibody conjugate to enable more of said antibody to bind with the antigens on the abnormal tissue, thereby increasing an uptake of the PEG/photosensitizer/antibody conjugate by the abnormal tissue; and

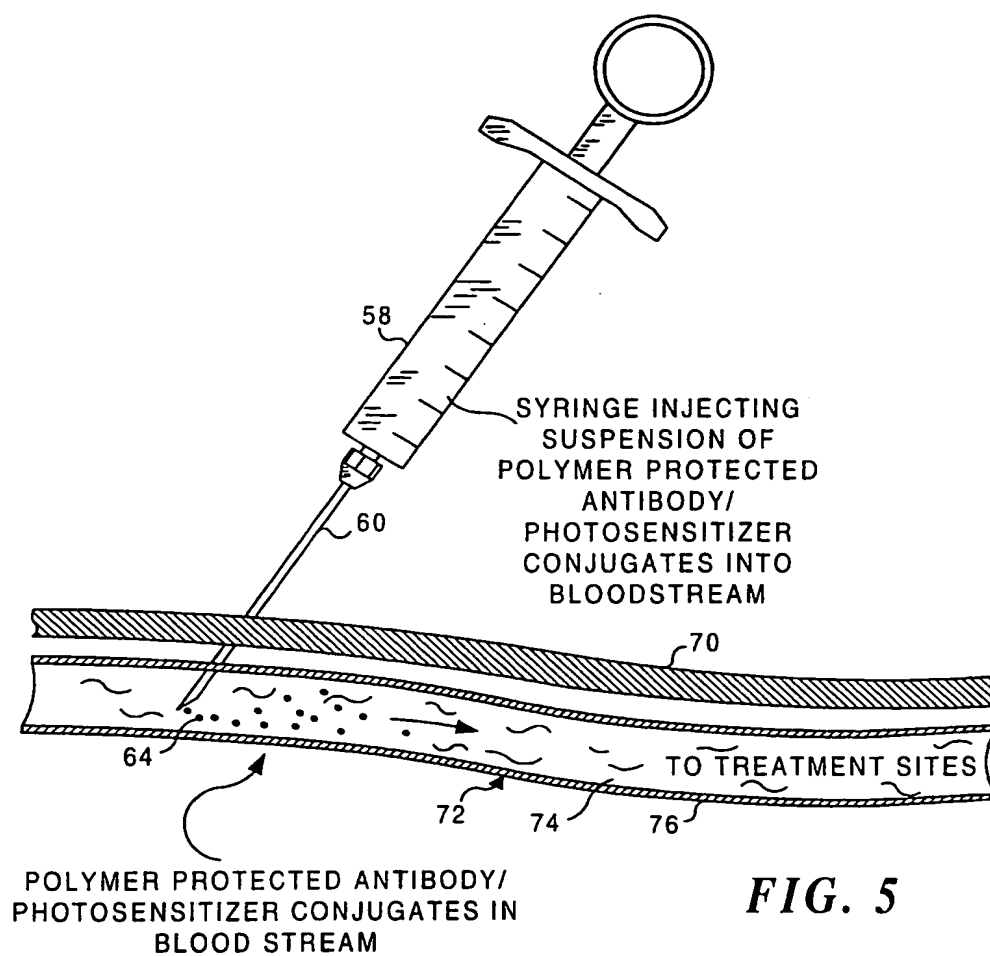
(b) after sufficient time has elapsed following administration of the PEG/photosensitizer/antibody conjugate to permit the antibody to bind with the antigens, administering a light therapy, said light therapy activating the photosensitizer and more effectively destroying the abnormal tissue due to the increased uptake of the PEG/photosensitizer/antibody conjugate by the abnormal tissue.

23. The method of Claim 22, wherein the PEG/photosensitizer/antibody conjugate comprises a microparticle of conjugated photosensitizer and antibody coated with said PEG.

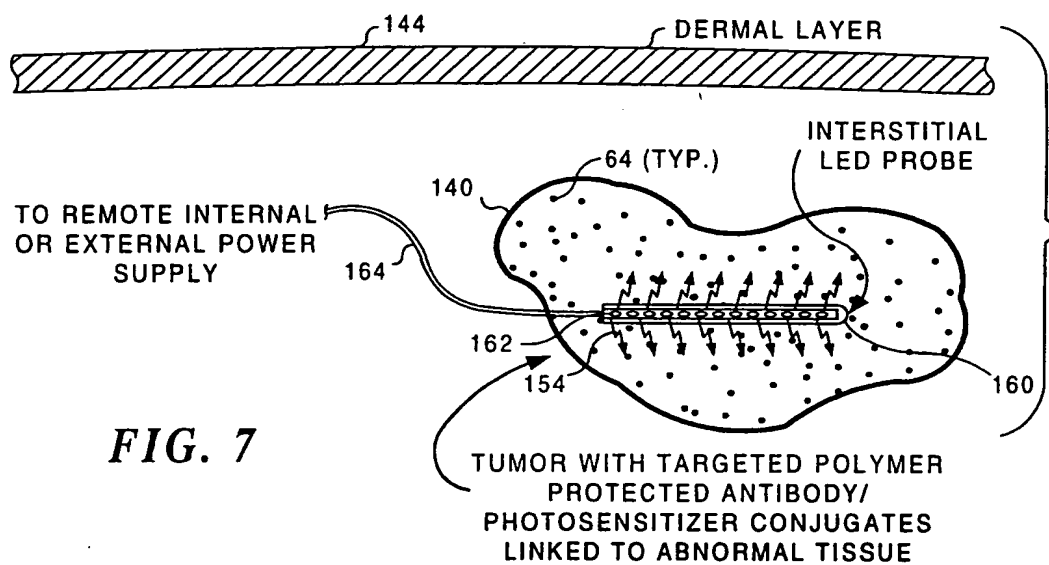
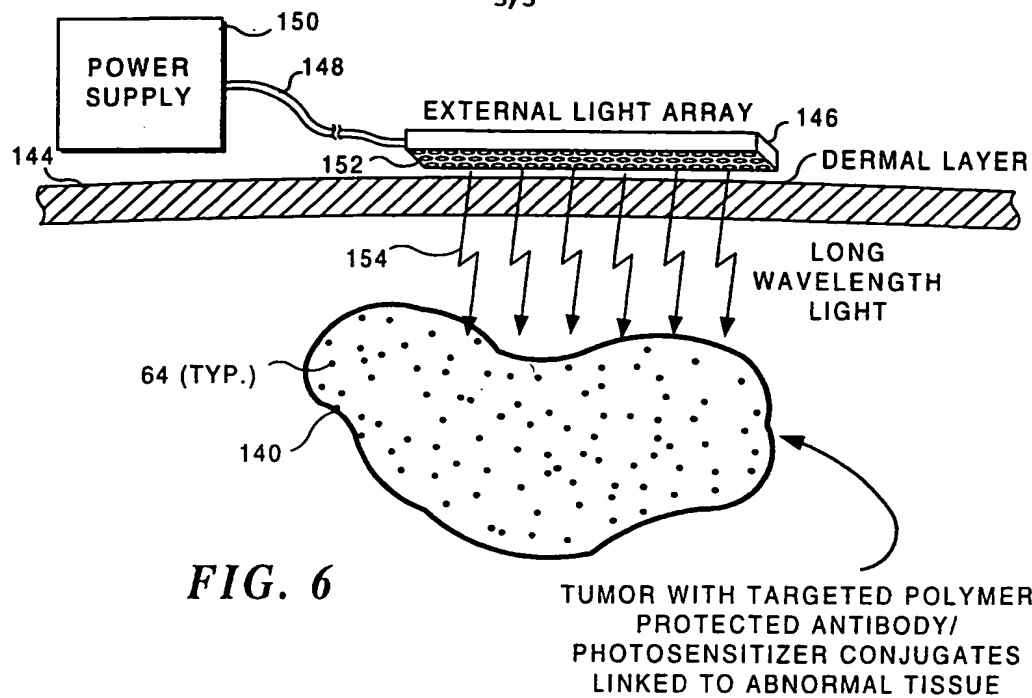
24. The method of Claim 22, wherein conjugated photosensitizer and antibody is covalently bonded to said PEG.

25. The method of Claim 22, wherein conjugated photosensitizer and antibody are covalently bonded to different sites on said PEG.



**FIG. 5**

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INTERNATIONAL SEARCH REPORT

International application No.
PCT/US99/20530

A. CLASSIFICATION OF SUBJECT MATTER

IPC(6) : A61B 17/36; A61K 31/40

US CL : 607.88

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 606-1-3, 10-12, 14-17; 607.88-90

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

WEST

Search via United States patent database.

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 5,308,608 A (DOLPHIN et al.) 03 May 1994, entire document.	1-6, 11-13, 15
---		7-10, 14, 17
Y		
Y	US 5,198,460 A (PANDEY et al.) 30 March 1993, entire document.	1-6, 8-13, 15, 17-19
A	US 5,611,793 A (WILSON et al.) 18 March 1997, entire document.	1-25
A	US 5,109,016 A (DIXON et al.) 28 April 1992, entire document.	1-25

☐ Further documents are listed in the continuation of Box C.☐ See patent family annex.

* Special categories of cited documents

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O document referring to an oral disclosure, use, exhibition or other means

P document published prior to the international filing date but later than the priority date claimed

T

later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

X

document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

Y

document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

Z

document member of the same patent family

Date of the actual completion of the international search

26 OCTOBER 1999

Date of mailing of the international search report

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